### Computational Modeling of Electrode with Saline Irrigation for **Radiofrequency Cardiac Ablation KBIOHEALTH** J. W. Ahn<sup>1</sup>, Y. J. Kim<sup>1</sup>, S. A. Lee<sup>1</sup>, H. C. Jung<sup>1</sup>, S. H. Lee<sup>1</sup>, J. H. Moon<sup>1\*</sup> 1. Osong medical innovation foundation, medical device development center,

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#### Introduction

 RadioFrequency Catheter Ablation(RFCA) is safe procedure to eliminate cardiac tissue caused arrhythmias.

•During RFCA, thrombus formation can occur if the electrode-tissue interface temperature reaches around 80°C[1].

•To prevent this phenomenon, the saline irrigable electrodes have been developed and can inject saline into blood-tissue interface through holes around electrode tip.

•We investigate the computational modeling electrode with saline irrigation including the flow problem about the blood circulation and the saline irrigation flow.

## **Boundary conditions**

•In velocity boundary conditions, inlet velocity boundary condition is applied on the left surface to impose a blood flow(  $U_{\rm f}=0.1m/s$ ).

•A constant temperature of 37 °C is fixed on the outer model surfaces.

proportional-integral(PI) implemented a •The model temperature control algorithm in the electrical boundary conditions( $K_P = 7, K_I = 5$ ).

## **Problem Definition**

- The problem we wish to solve is the temperature distribution of cardiac tissue, electrode and blood when the saline is injected through the electrode including 6 irrigation holes.
- The thermal lesions are identified by the 50 °C isotherm contour and determined by their characteristic dimensions: Maximum depth(D), maximum width(MW), depth at the maximum width(DW)[2].



•The temperature of measure point is electrode-tissue interface and called "set temperature".

•The value of  $T_{set}$  is 50, 45, 40, 35°C.



**Figure 2**. Boundary conditions of the numerical model.

#### Results

•When the set temperature is increased, the size of the thermal lesion and the maximum temperature show a increase regardless of the flow rate of the saline irrigation.

•In case of the constant set temperature, the thermal lesion show a increase due to convective heat transfer between electrode and saline irrigation flow if the flow rate of saline irrigation is increased.

## **Computational Methods**

•The numerical model is based on a coupled electric-thermal-flow problem.

•To solve the coupled problems, we use AC/DC Module, Heat Transfer Module, and CFD Module in COMSOL Multiphysics® software

•The thermal problem – Energy equation

$$\rho c_P \frac{\partial T}{\partial t} = \nabla \cdot (k \nabla T) + q - Q_p + Q_m - \rho c \boldsymbol{u} \cdot \nabla T$$

•Fluid flow problem – Navier-Stokes equation

$$\rho \frac{\partial \boldsymbol{u}}{\partial t} + \rho \boldsymbol{u} \cdot \nabla \boldsymbol{u} = -\nabla P + \mu \nabla^2 \boldsymbol{u} + \boldsymbol{F}$$
$$\rho \nabla \cdot \boldsymbol{u} = 0$$

•The electrical problem – Maxwell equation



**Figure 3**. The results of the temperature distribution of 3D model and the thermal lesion.

## Conclusions

•To prevent the temperature of cardiac tissue from exceeding 80°C, the set temperature of the electrode tip must be set differently according to the flow rate of the saline irrigation.

•We need to study more the model by varying the contact angle between the electrode and the cardiac tissue.



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